

FFR_{CT}: Beyond FFR

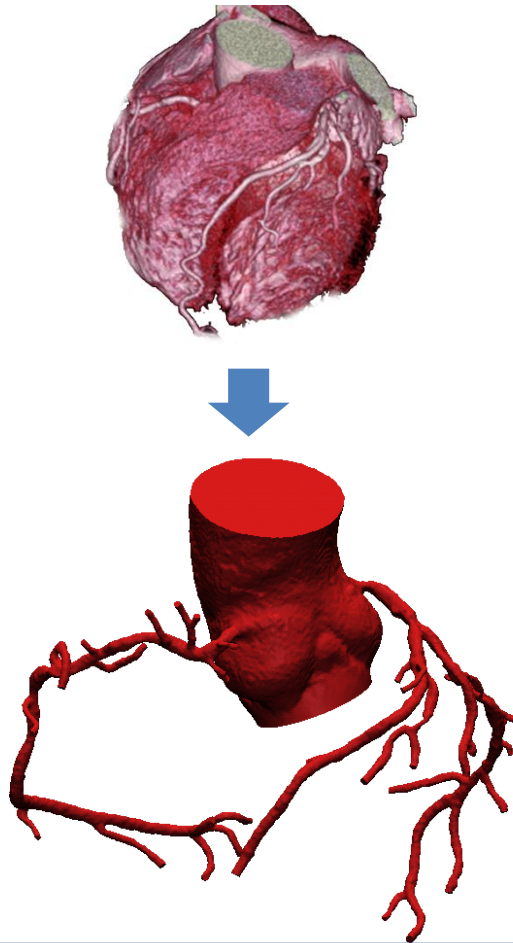
Bon-Kwon Koo, MD, PhD

Seoul National University Hospital, Seoul, Korea



Patient-specific non-invasive coronary hemodynamic assessment

Non-invasive, Pt-specific



Hemodynamics

- **Pressure**
 - Pressure difference
 - Pressure gradient
 - Pressure recovery
 - **FFR**
 - Flow velocity
 - Flow rate
 - Shear rate
 - Shear stress – average, peak, gradient
 - Traction
 - Oscillatory shear index
 - Particle residence time
 - Turbulent kinetic energy
 -
- Static
 - Pulsatile
 - Resting
 - Hyperemic
 - Exercise – mild, moderate, peak

Non-invasive hemodynamic parameter measurement using computational fluid dynamics and cCTA

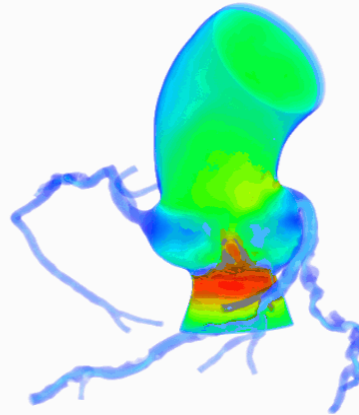


Rest

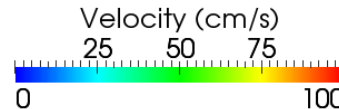
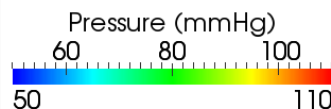
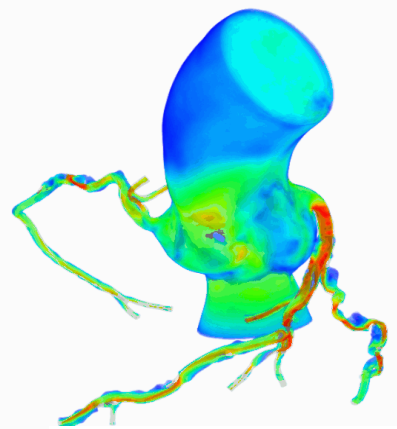
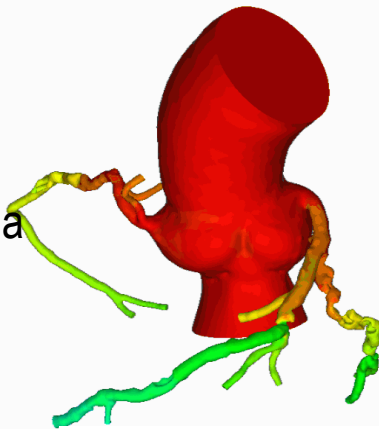
Pressure



Velocity



Hyperemia



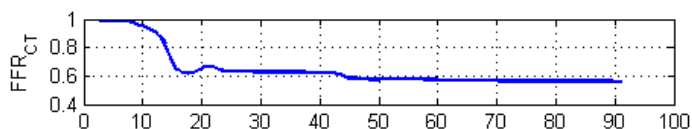
Hemodynamics

- Pressure
 - Pressure difference
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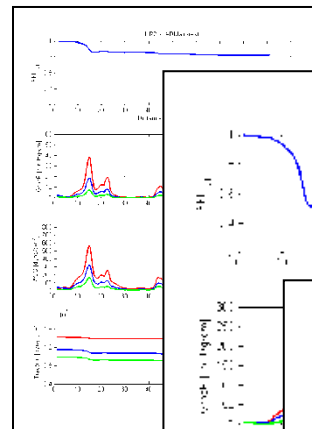
Image-based computerised modelling of coronary circulation: *Potentials*



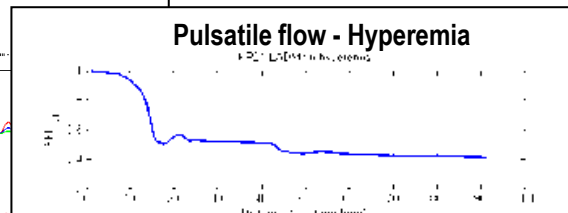
Static flow - hyperemic



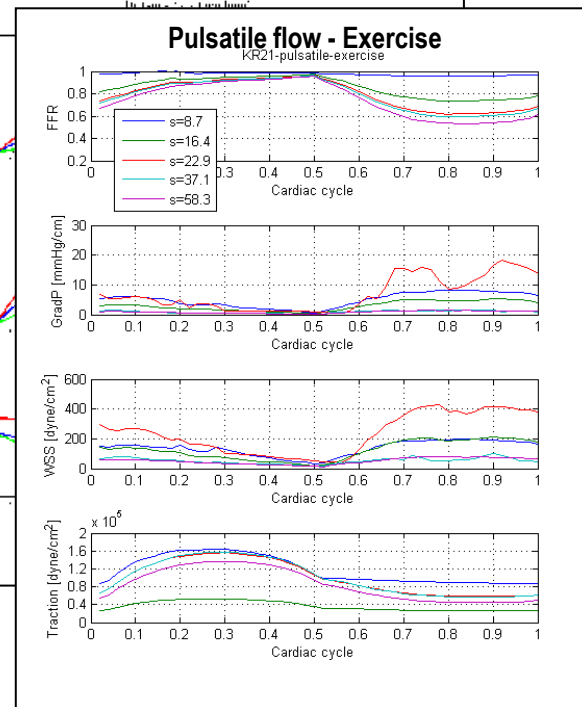
Pulsatile flow - rest



Pulsatile flow - Hyperemia

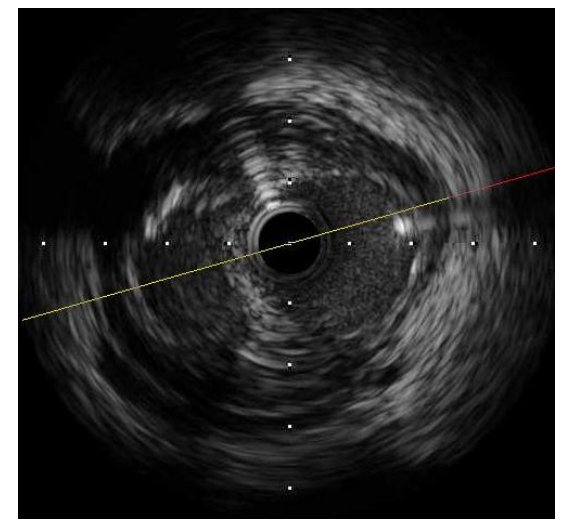
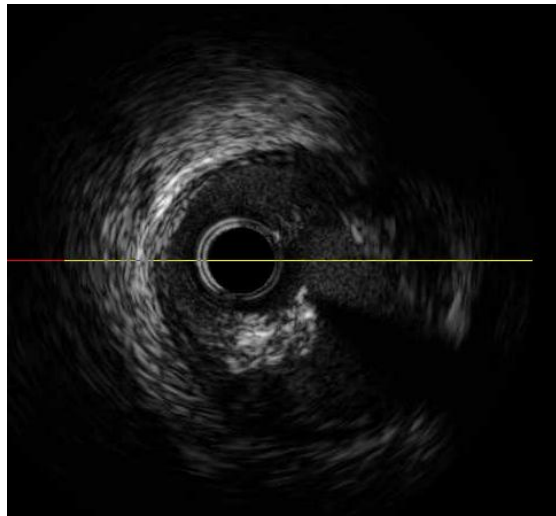
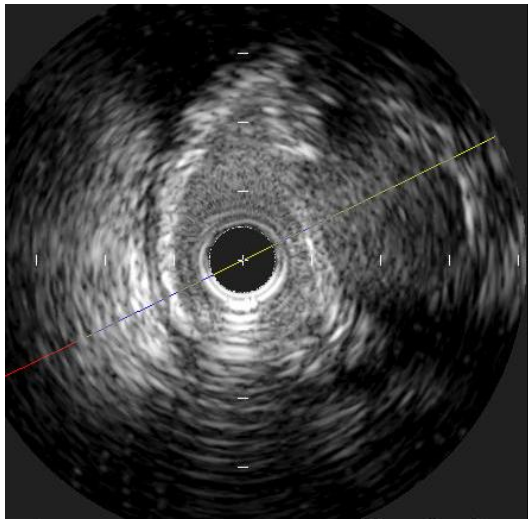


Pulsatile flow - Exercise



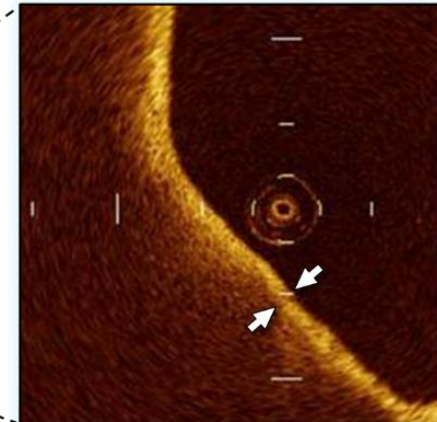
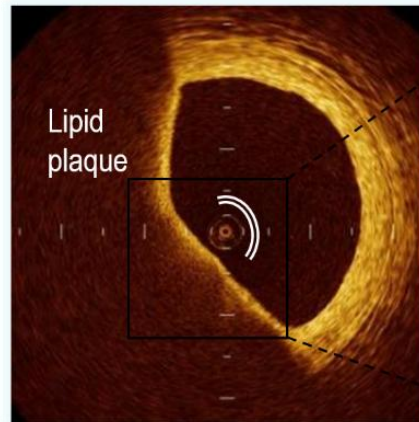
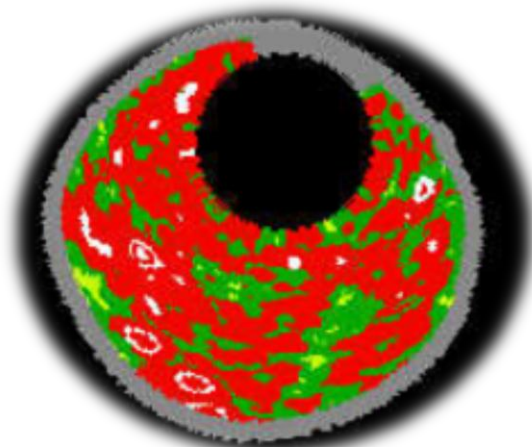
Why Does the Plaque Rupture?

Mechanistic link between Hemodynamics and Acute Coronary Syndrome



We already know....

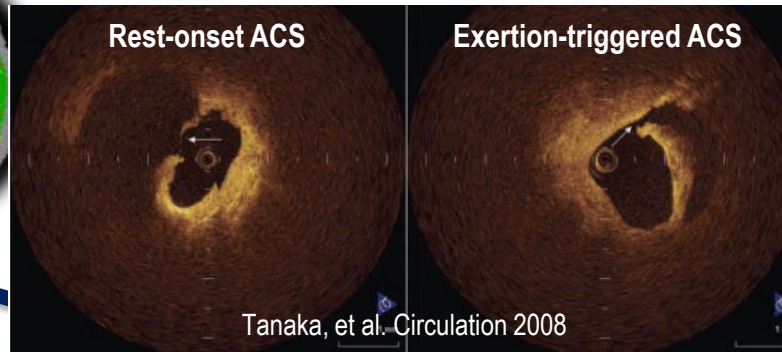
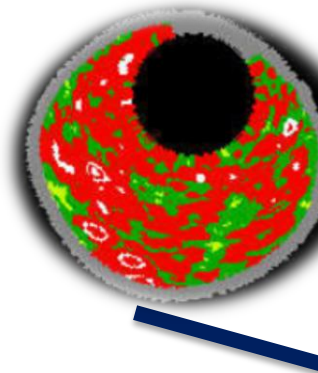
- Coronary plaque rupture is a critical event that triggers the initiation of acute coronary syndrome (ACS).
- Risk assessment for ACS
 - **Plaque Vulnerability:** cap thickness, lipid core, inflammation, neovascularization, posterior attenuation.....



Why does the plaque rupture?

:Mechanism of material failure

Durability = Vulnerability



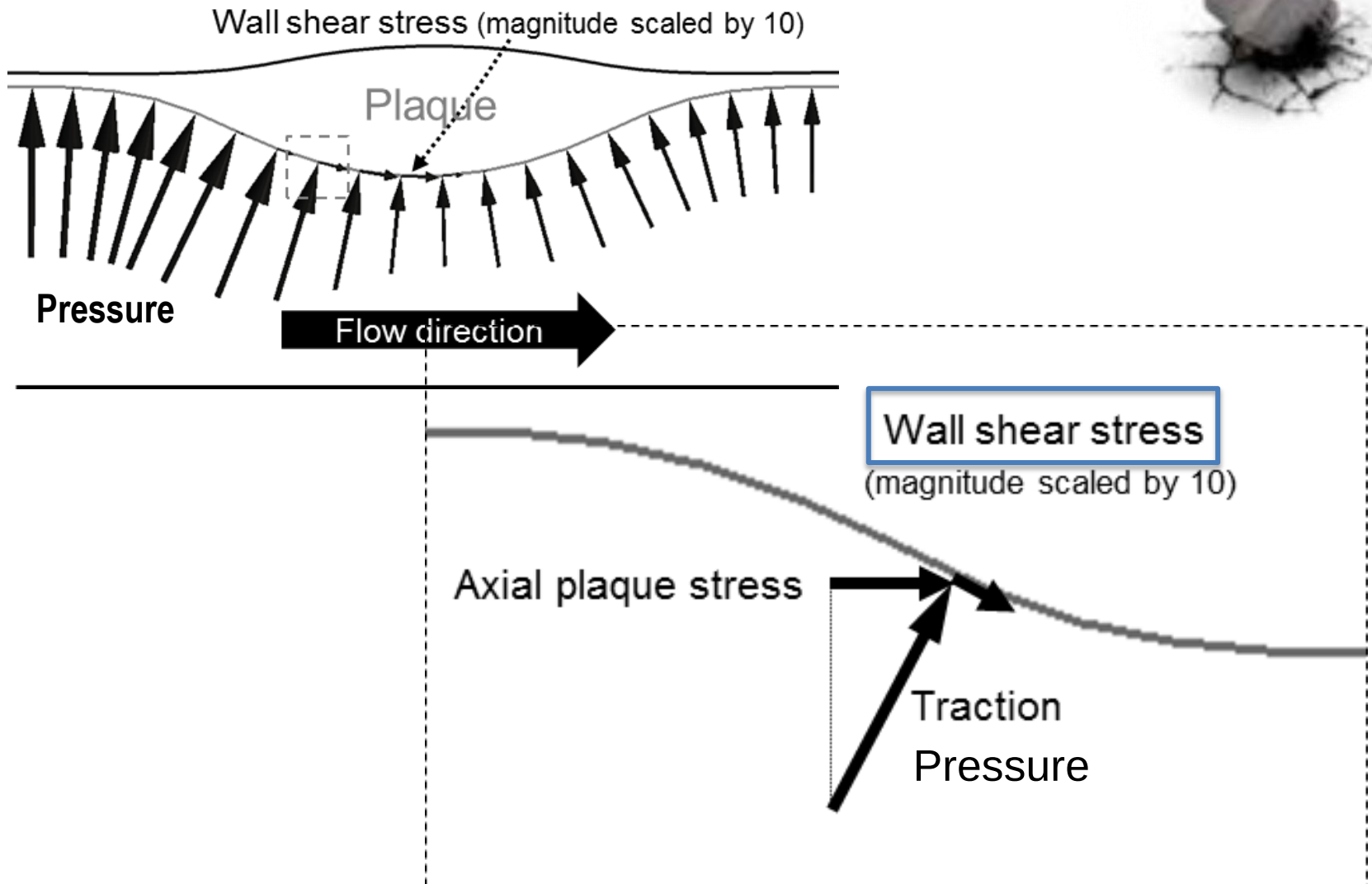
The broken cap was much thinner in the rest-onset group than in the exertion group (50 vs. 90 μm , $P < 0.01$)



External force

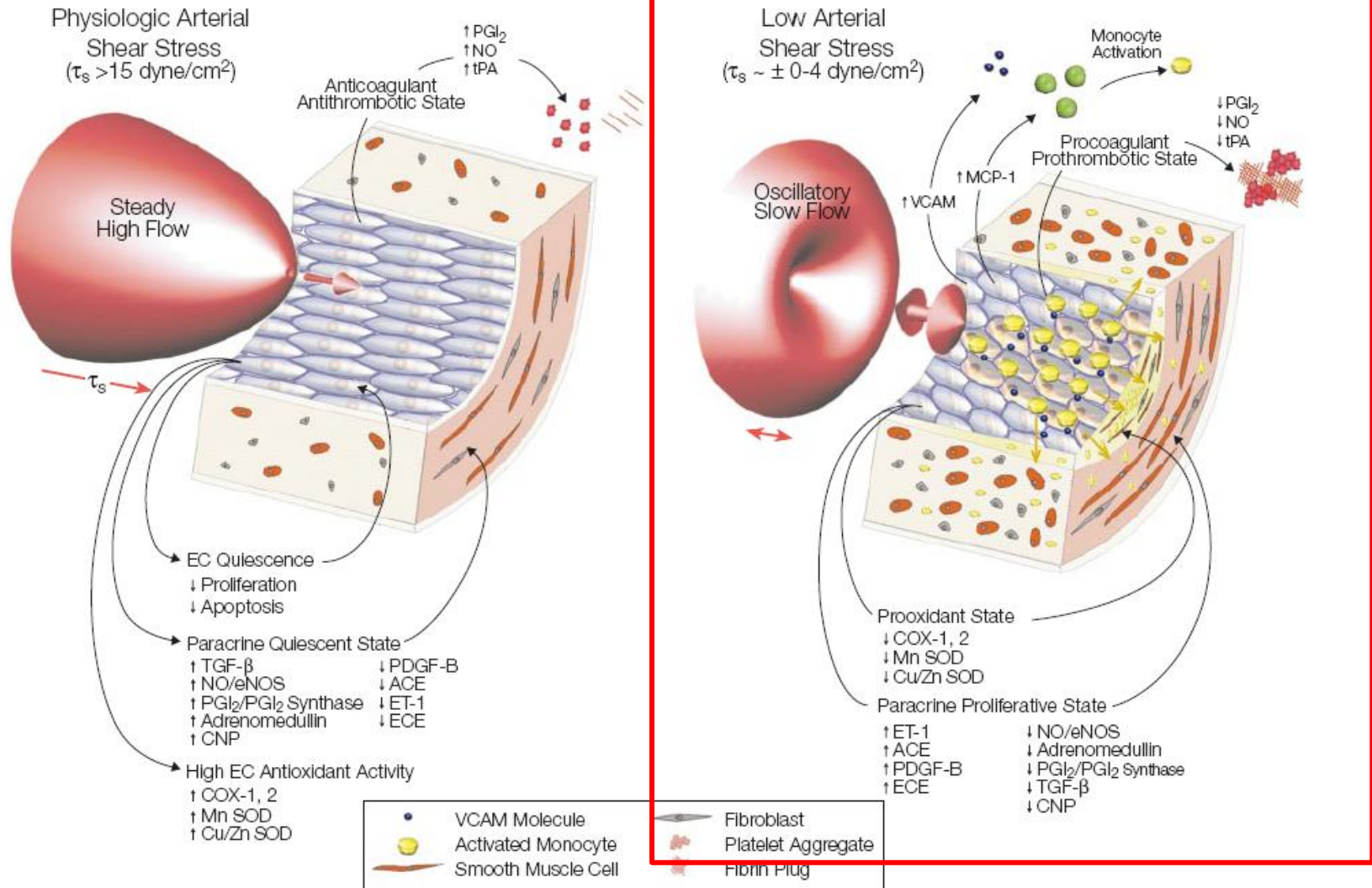
Information on external force in addition to vulnerability can lead to better discrimination of the risk of plaque rupture.

What kind of forces are acting on the plaque?



Low wall shear stress

→ Proliferative, pro-inflammatory, pro-thrombotic stimulus



Very high WSS vs. Vulnerability

Annals of Biomedical Engineering, Vol. 41, No. 7, July 2013 (© 2012) pp. 1411–1427
DOI: 10.1007/s10439-012-0695-0

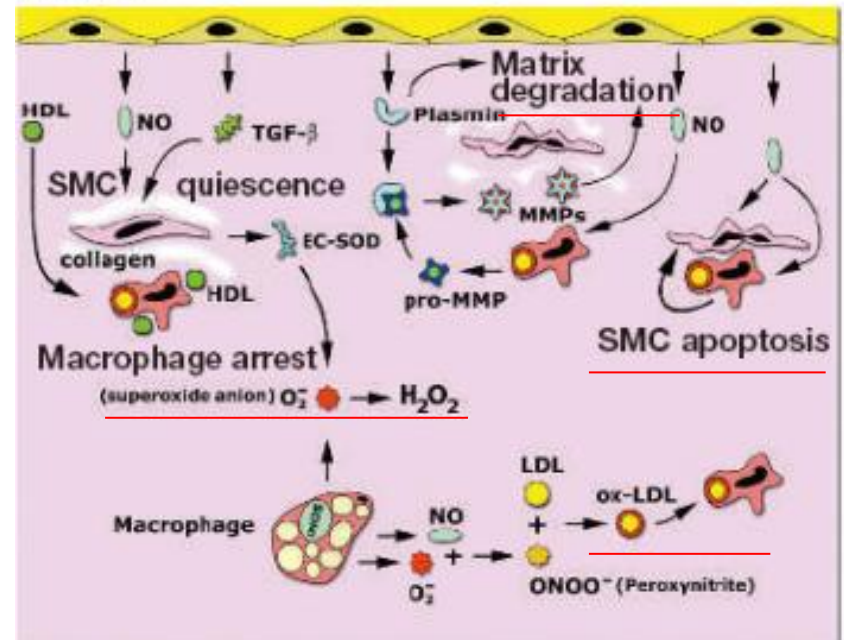


High Wall Shear Stress and Spatial Gradients in Vascular Pathology: A Review

JENNIFER M. DOLAN,^{1,3,4} JOHN KOLEGA,^{1,3,4} and HUI MENG^{1,2,3,5}

Very High SS

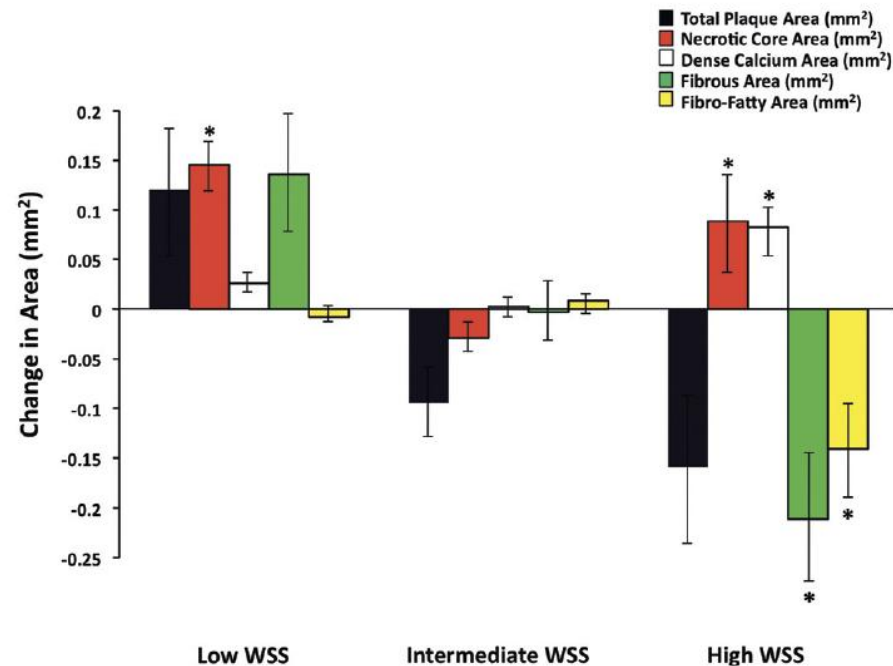
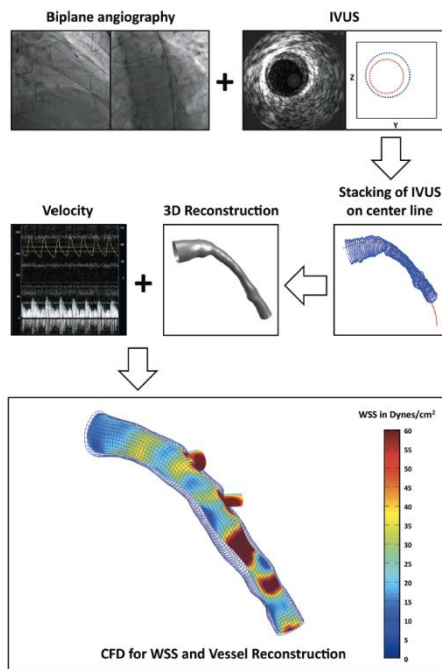
Abstract—Cardiovascular pathologies such as intracranial aneurysms (IAs) and atherosclerosis preferentially localize to bifurcations and curvatures where hemodynamics are complex. While extensive knowledge about low wall shear stress (WSS) has been generated in the past, due to its strong relevance to atherogenesis, high WSS (typically > 3 Pa) has emerged as a key regulator of vascular biology and pathology as well, receiving renewed interests. As reviewed here, chronic high WSS not only stimulates adaptive outward remodeling, but also contributes to saccular IA formation (at bifurcation apices or outer curves) and atherosclerotic plaque destabilization (in stenosed vessels). Recent advances in understanding IA pathogenesis have shed new light on the



Slager, et al. Nature Clin Pract 2005

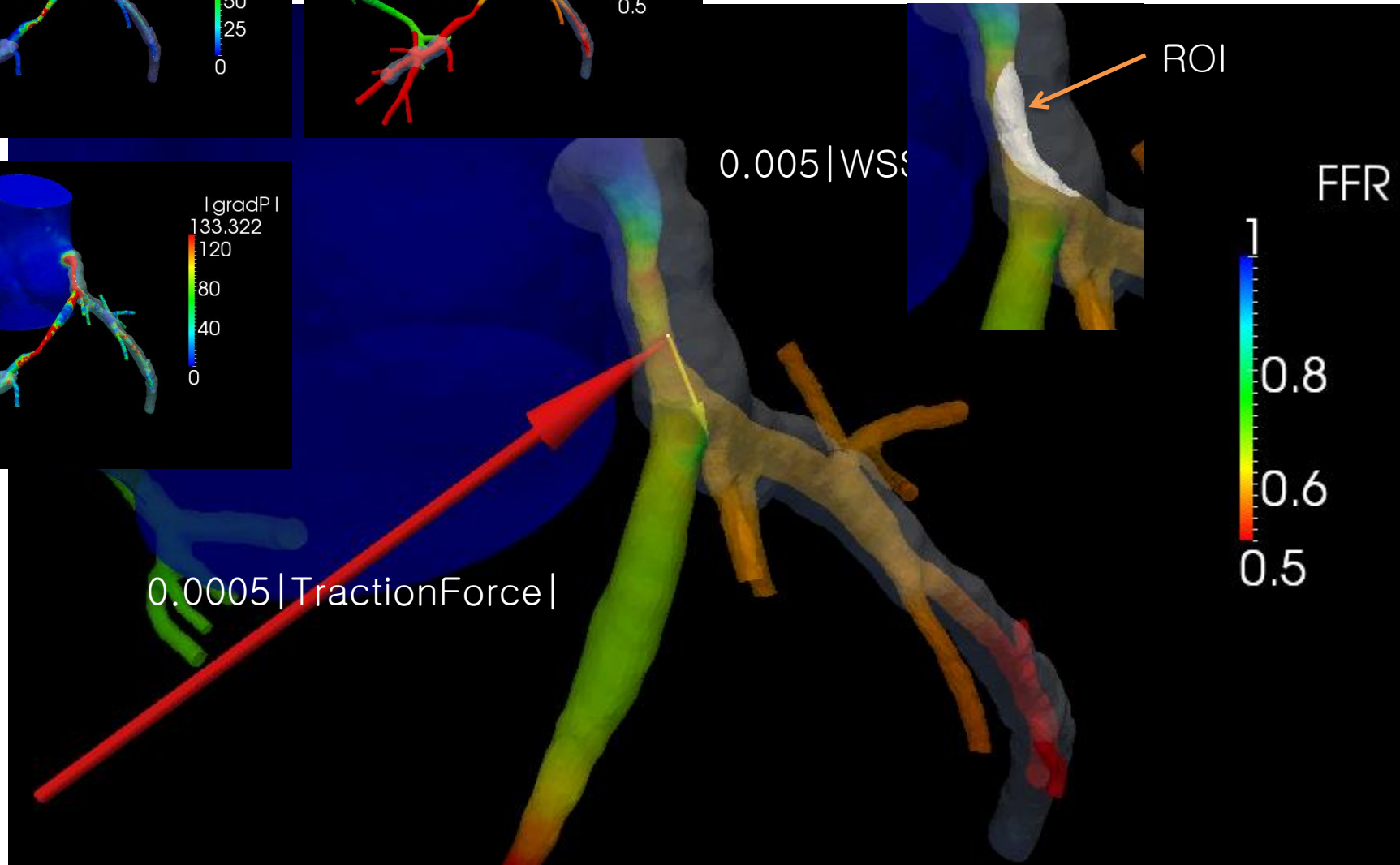
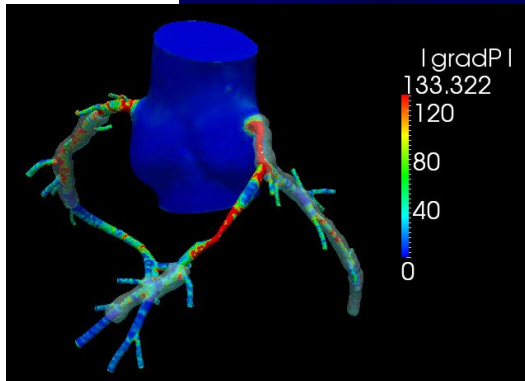
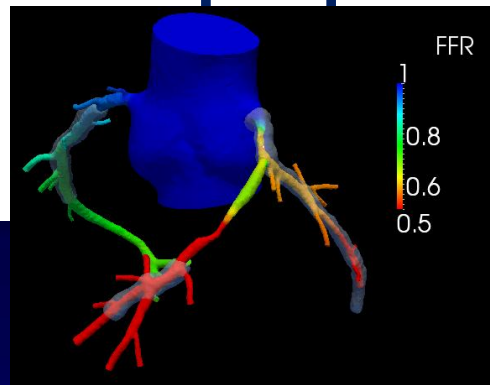
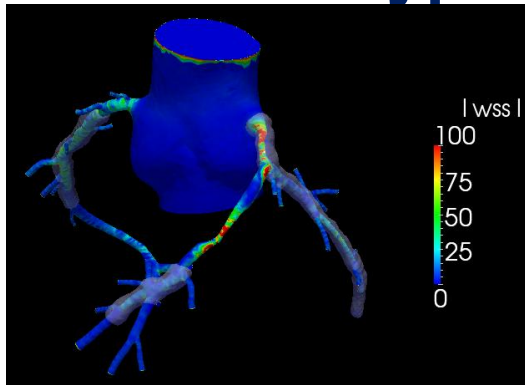
Coronary Artery Wall Shear Stress Is Associated With Progression and Transformation of Atherosclerotic Plaque and Arterial Remodeling in Patients With Coronary Artery Disease

Habib Samady, MD; Parham Eshtehardi, MD; Michael C. McDaniel, MD; Jin Suo, PhD; Saurabh S. Dhawan, MD; Charles Maynard, PhD; Lucas H. Timmins, PhD; Arshed A. Quyyumi, MD; Don P. Giddens, PhD

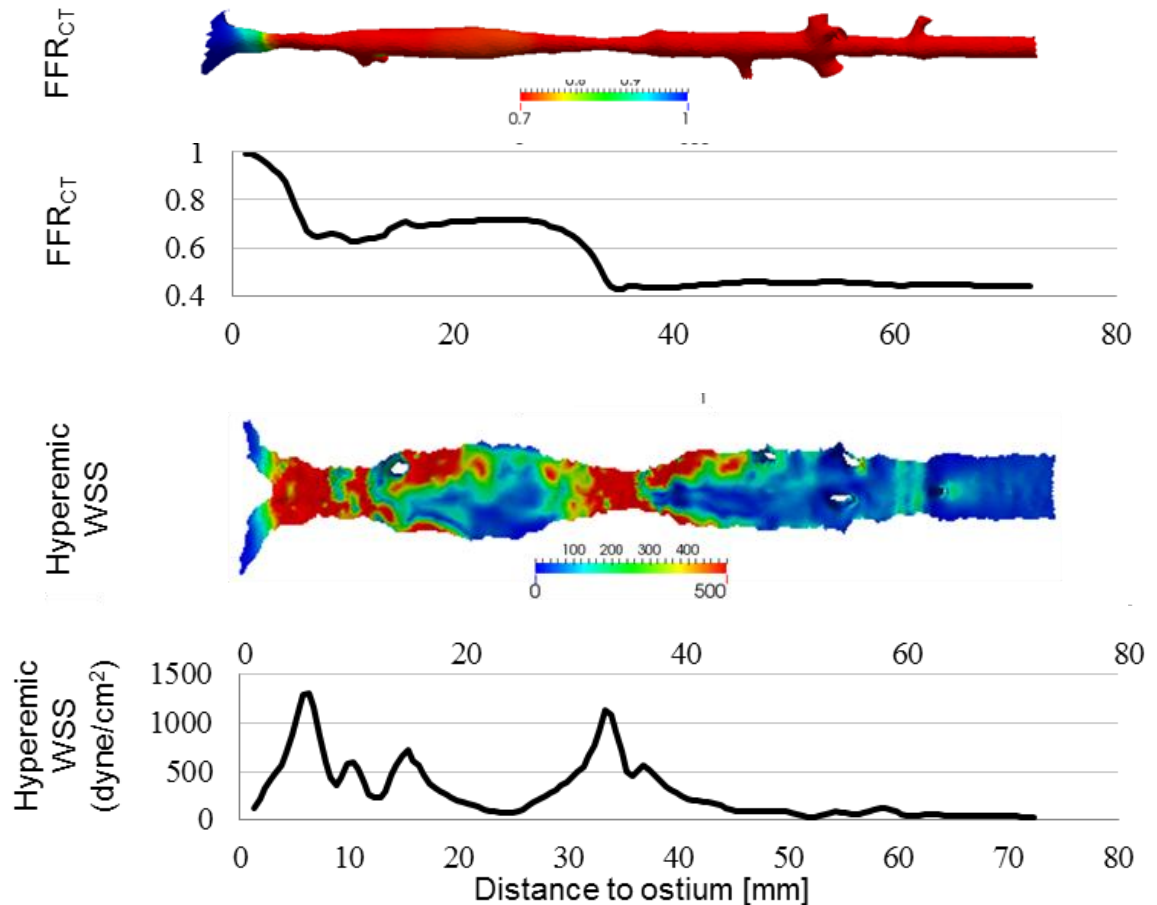


Conclusions—Compared with intermediate-WSS coronary segments, low-WSS segments develop greater plaque and necrotic core progression and constrictive remodeling, and high-WSS segments develop greater necrotic core and calcium progression, regression of fibrous and fibrofatty tissue, and excessive expansive remodeling, suggestive of transformation to a more vulnerable phenotype.

Prototype: Total plaque force model (May 29, 2013)

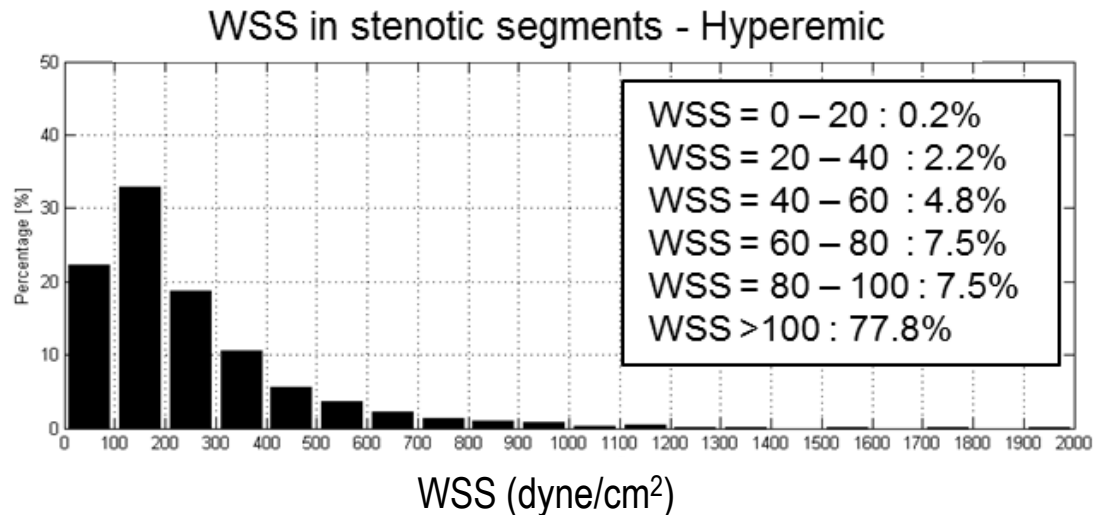
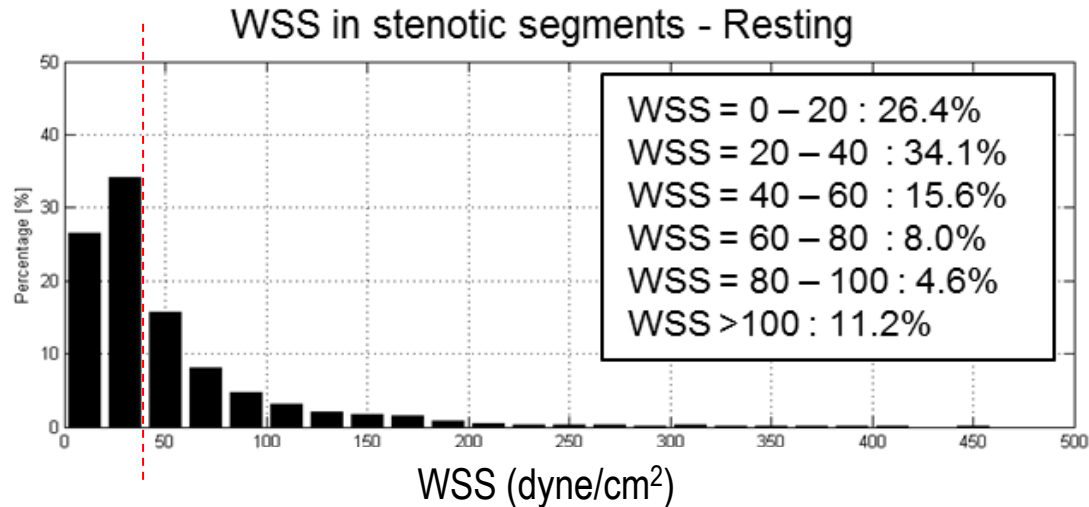


Measurement of hemodynamic parameters in a patient using cCTA and computational fluid dynamics

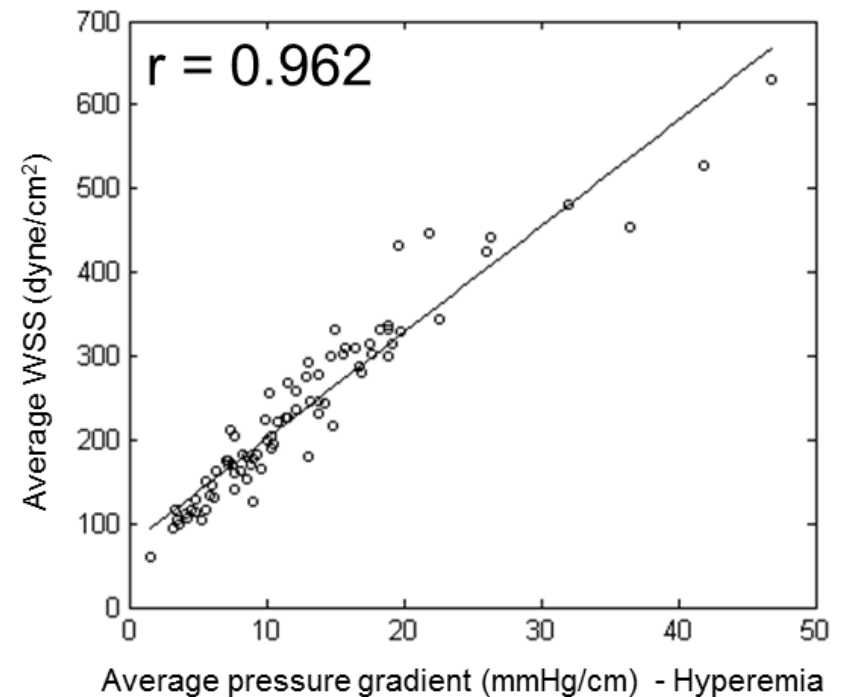
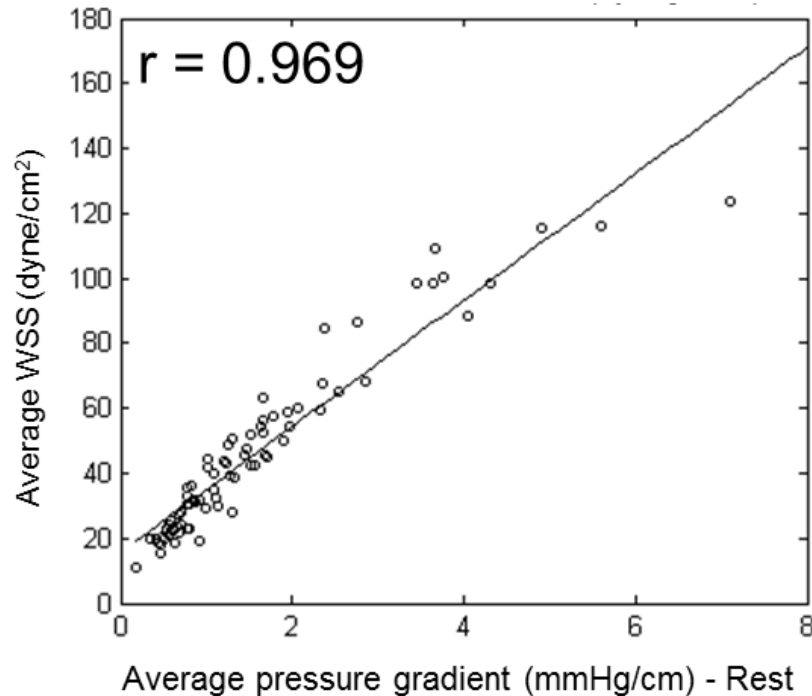


WSS in clinically relevant lesions

- 80 patients
- Clinically driven invasive coronary angiography and CT angiography
- Average % diameter stenosis: $52.3 \pm 12.4\%$

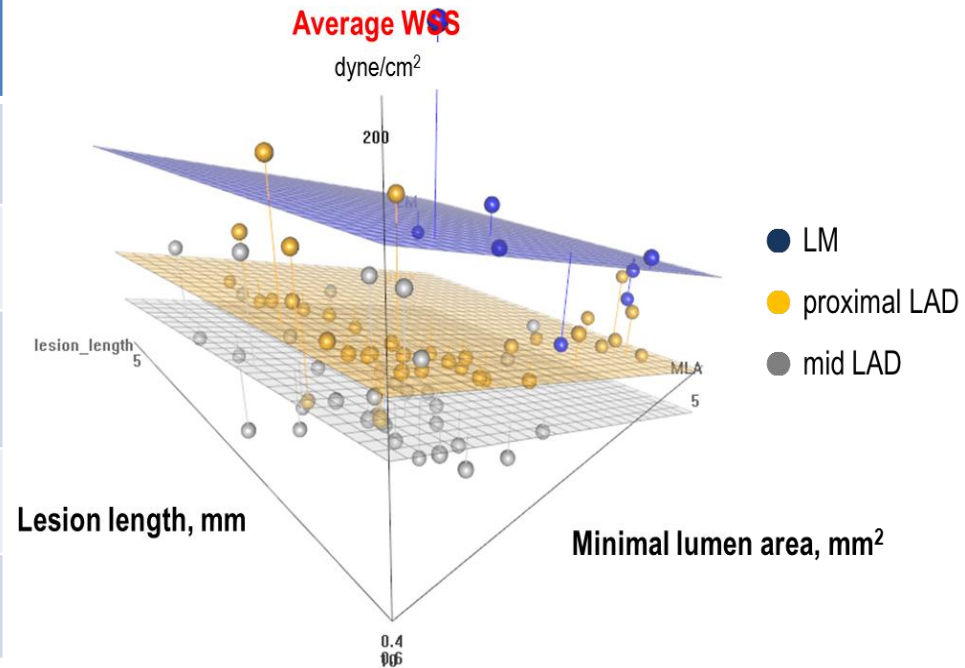


Relationship between WSS and pressure gradient

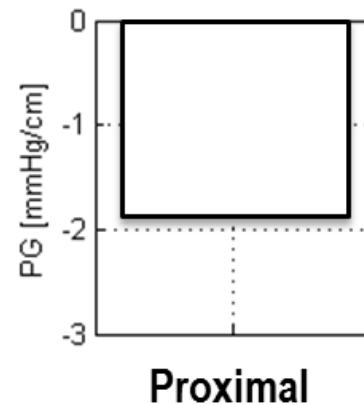
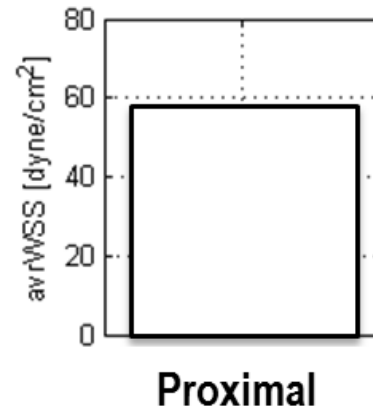
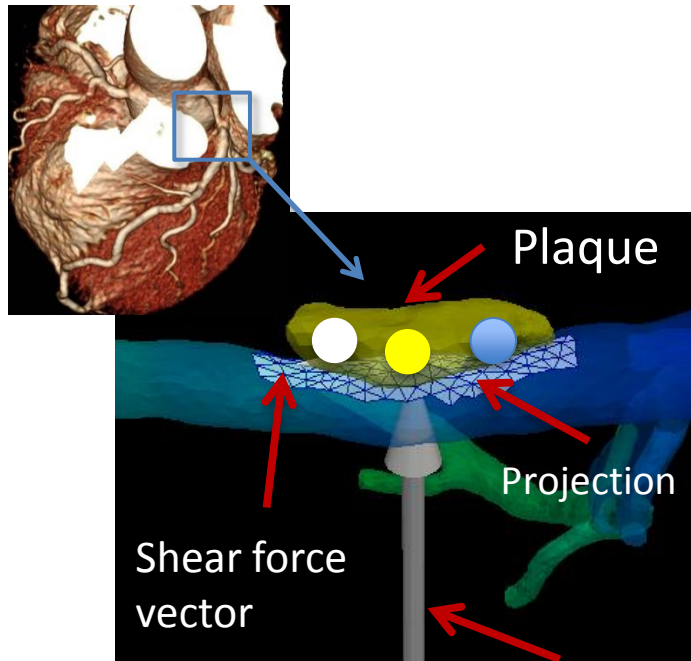


Relationship between WSS and lesion characteristics

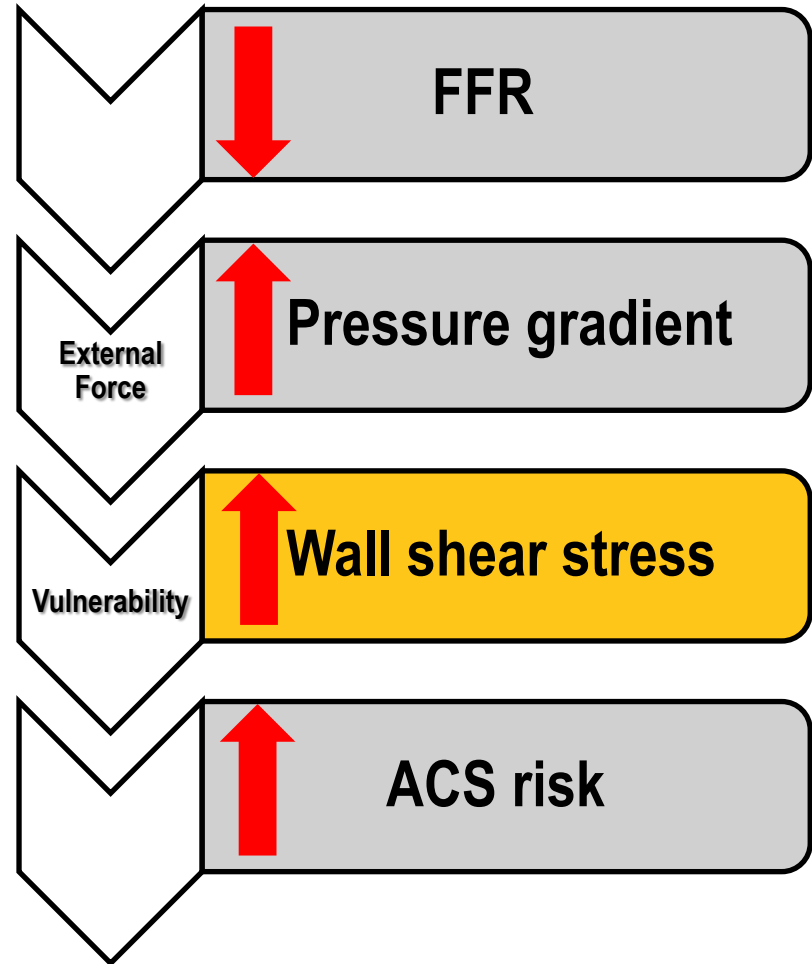
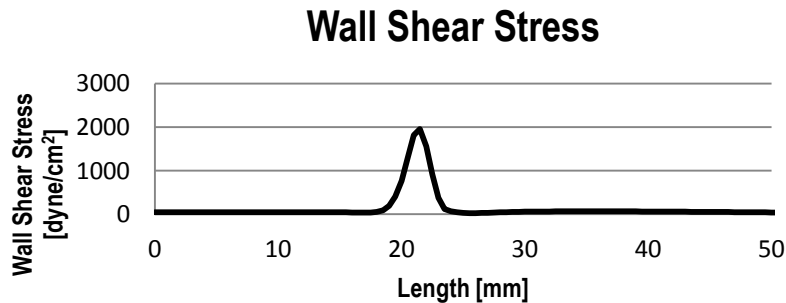
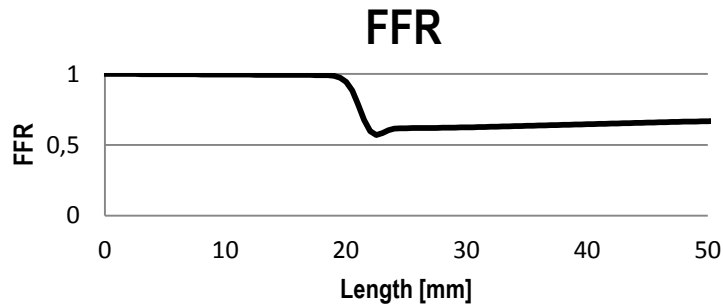
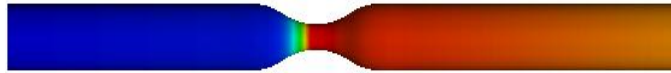
Determinants	β	95% CI	p
Pressure Gradient	1.281	0.35 – 2.25	0.007
Blood flow	0.683	0.34 – 1.02	<0.001
Distance from LM ostium	-0.298	-0.56 – -0.04	0.024
Minimal lumen area	-1.676	-2.44 – -0.92	<0.001
Lesion length	-1.157	-1.81 – -0.51	<0.001



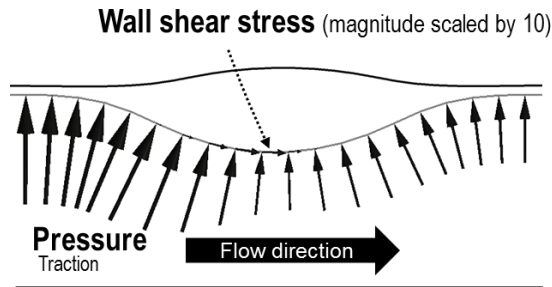
Regional distribution of hemodynamic forces : Pressure gradient vs. WSS



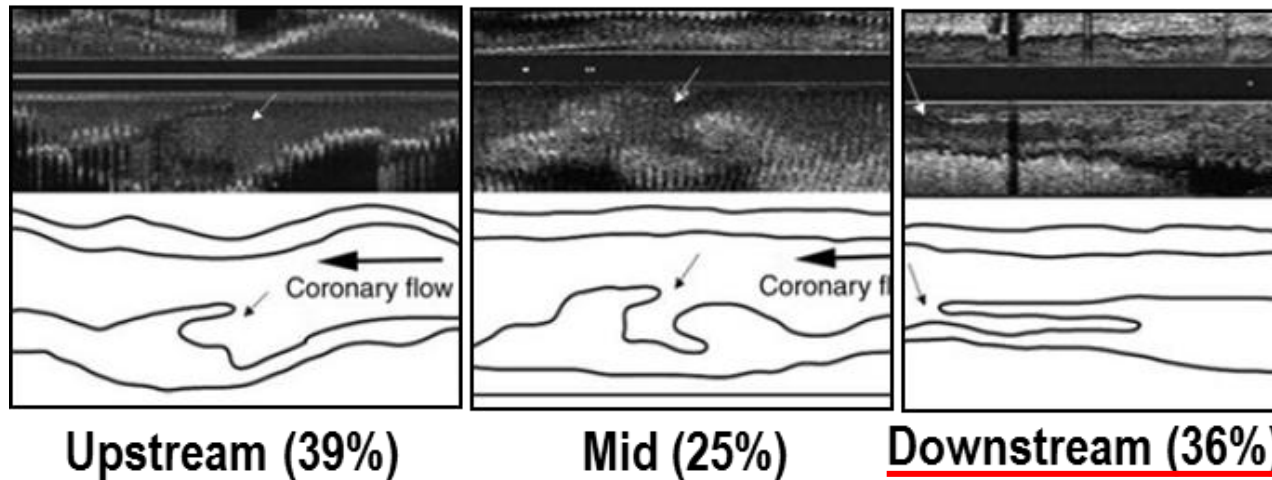
FFR vs. ACS



WSS and pressure, are they enough?



Location of rupture



Tanaka, et al. Eur Heart J 2008;29:38-44

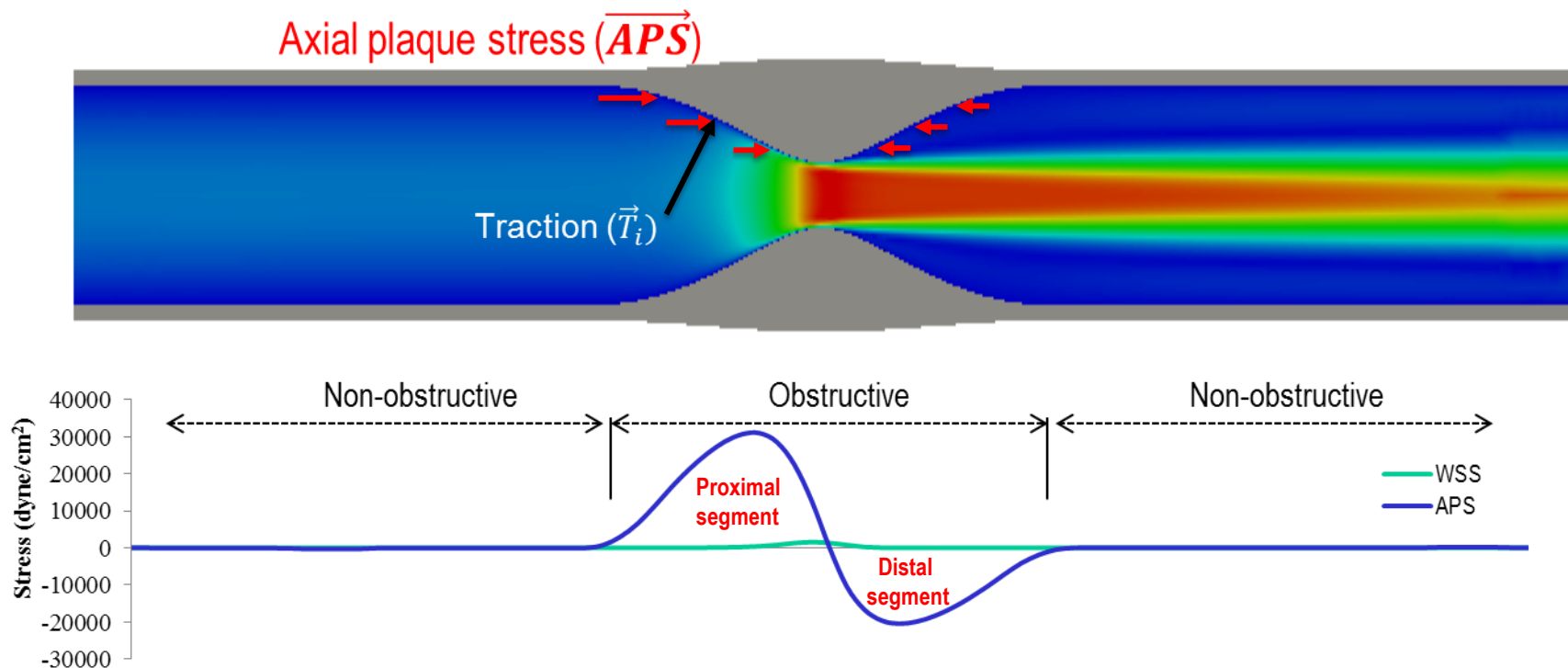
Pressure, FFR and WSS are high at the upstream segment of a plaque. Therefore, these parameters cannot explain the occurrence of downstream rupture.

WSS and pressure, then what else?

- Traction is the total force (stress) acting on vessel wall (plaque), and can be decomposed

In relation to lumen surface: $\|\mathbf{Traction}\|^2 = \|\mathbf{WSS}\|^2 + \|\mathbf{Pressure}\|^2$

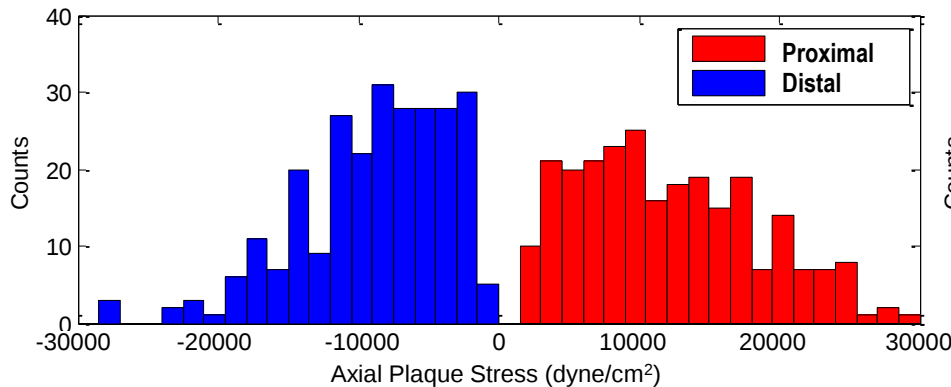
In relation to centerline: $\|\mathbf{Traction}\|^2 = \|\mathbf{Axial Stress}\|^2 + \|\mathbf{Radial Stress}\|^2$



Axial plaque stress is much larger than WSS and uniquely characterizes the upstream and downstream segments of coronary stenosis.

Distribution of “Axial Plaque Stress”

Idealized stenosis models (n=264)



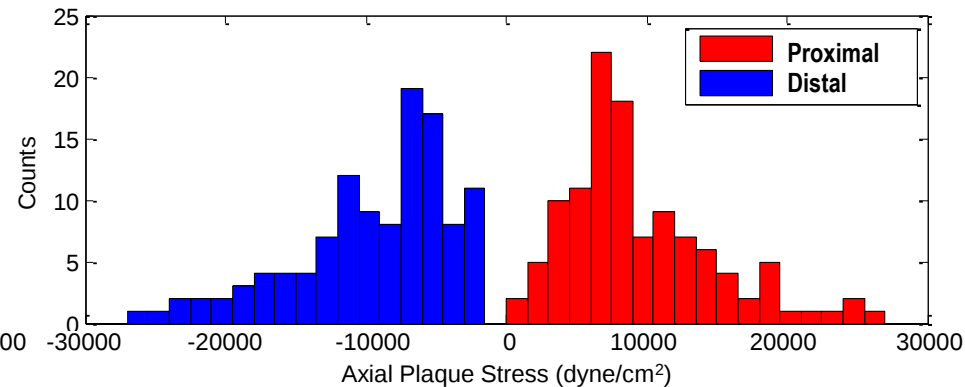
Distal segment

- N=264
- Median: -7801.3 dyne/cm²
- IQR: -11954.3, -4603.1

Proximal segment

- N=264
- Median: 11629.4 dyne/cm²
- IQR: 11954.3, 4603.2

Patients' lesions (n=114)



Distal segment

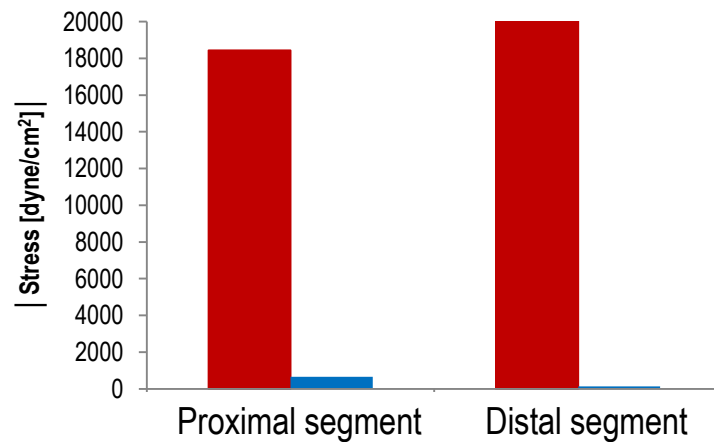
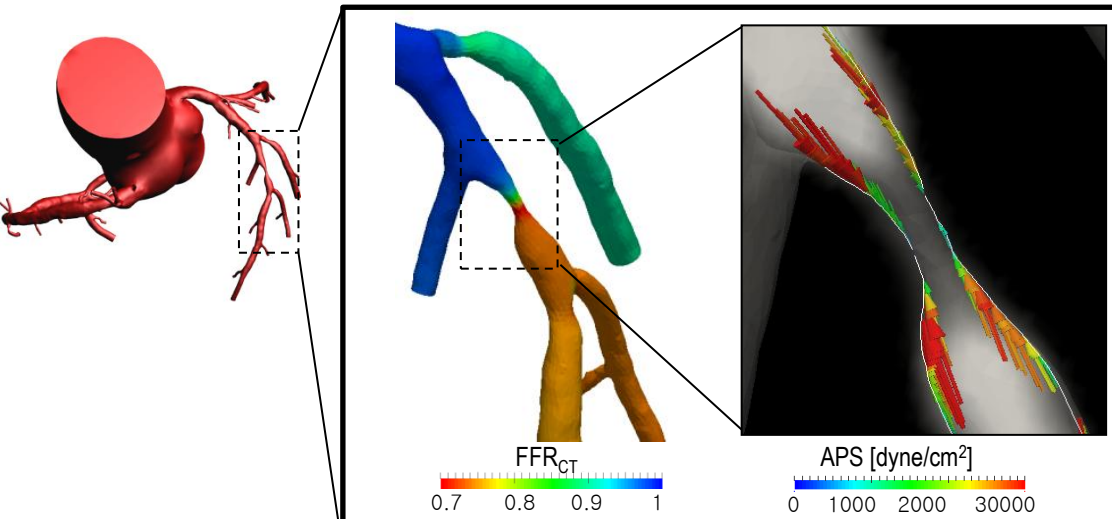
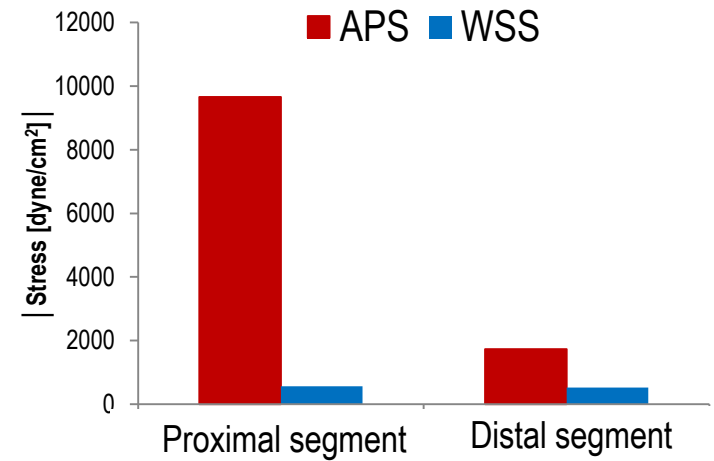
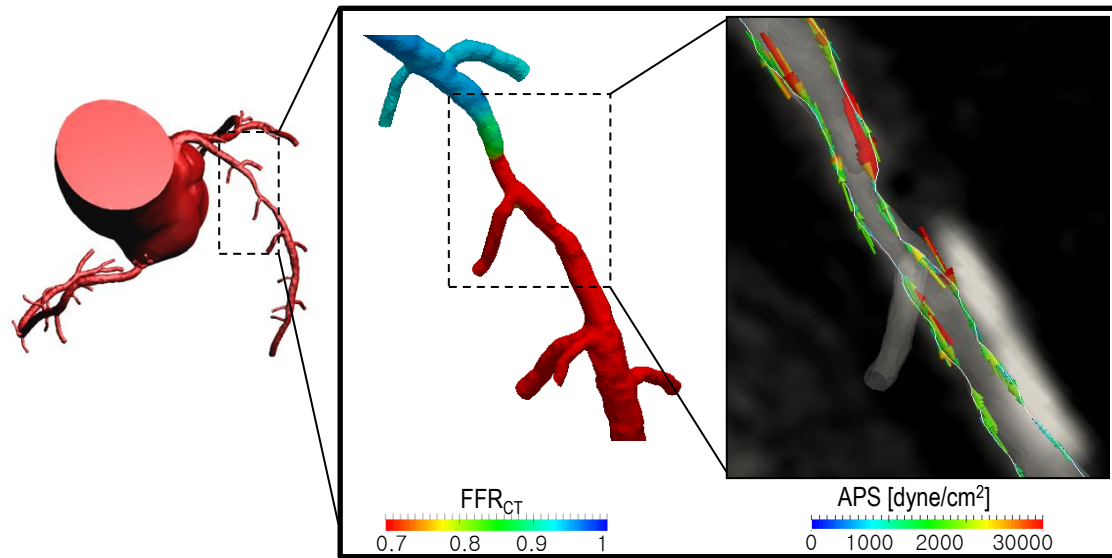
- N=114
- Median: -7912.4 dyne/cm²
- IQR: -12366.7, -5632.7

Proximal segment

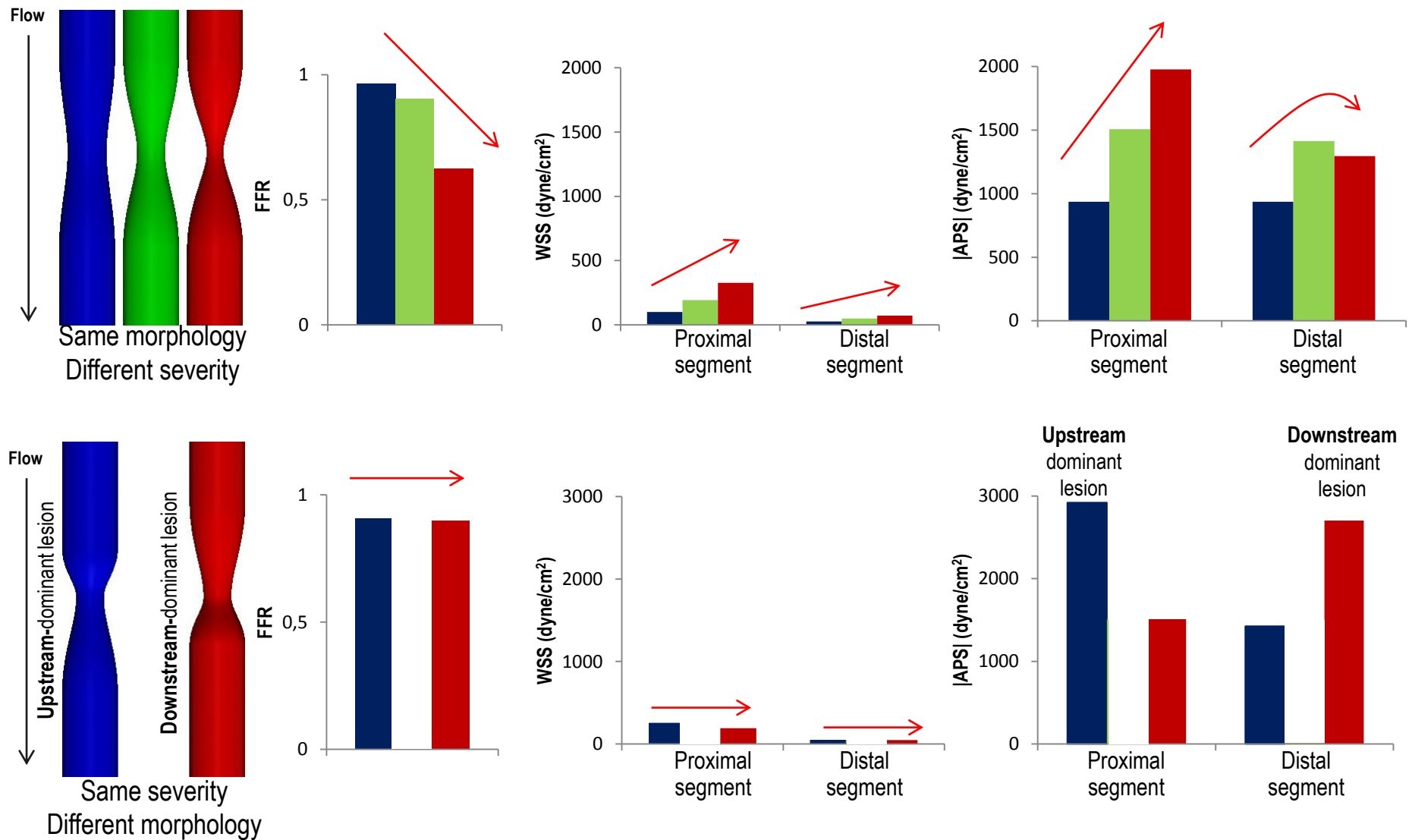
- N=114
- Median: 7885.66 dyne/cm²
- IQR: 6055.9, 12707.9

Distribution of axial plaque stress is similar between idealized models and patients lesions.

Distribution of Axial Plaque Stress in patients



Lesion geometry vs. Hemodynamic forces



Influence of “Lesion Shape” on Hemodynamic Parameters (n=114)

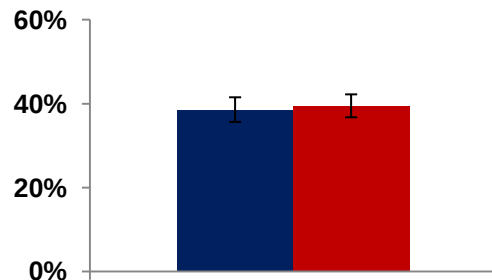


Upstream-dominant lesion
(n=56)

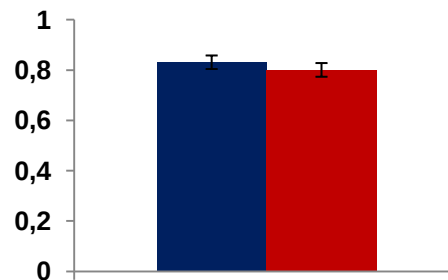


Downstream-dominant lesion
(n=58)

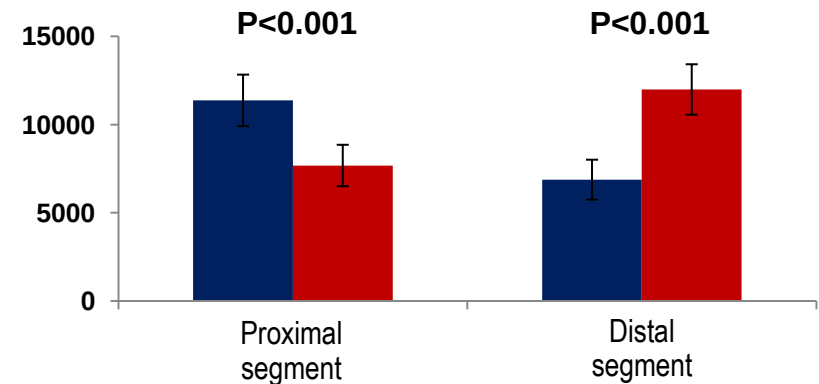
% Diameter Stenosis



FFR_{CT}



| Axial Plaque Stress | (dyne/cm²)

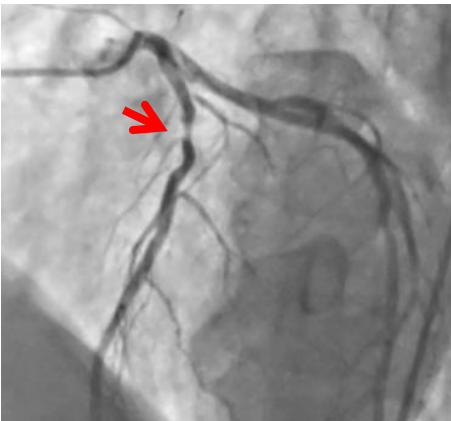


Future perspective

2011-04 CT, Asymptomatic

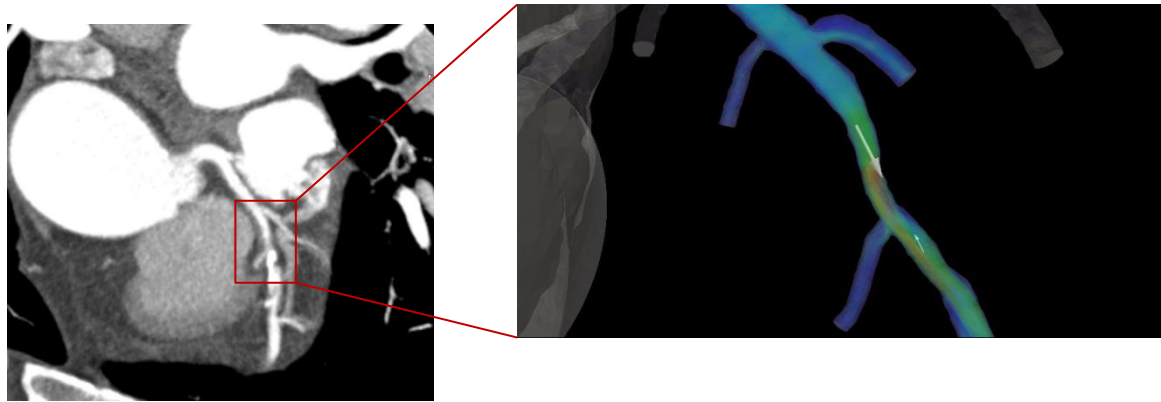


2012-06 Acute MI

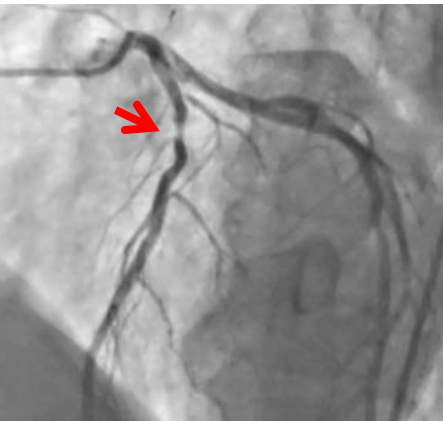


Future perspective

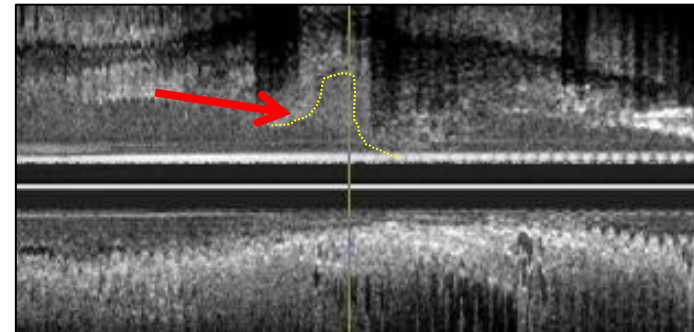
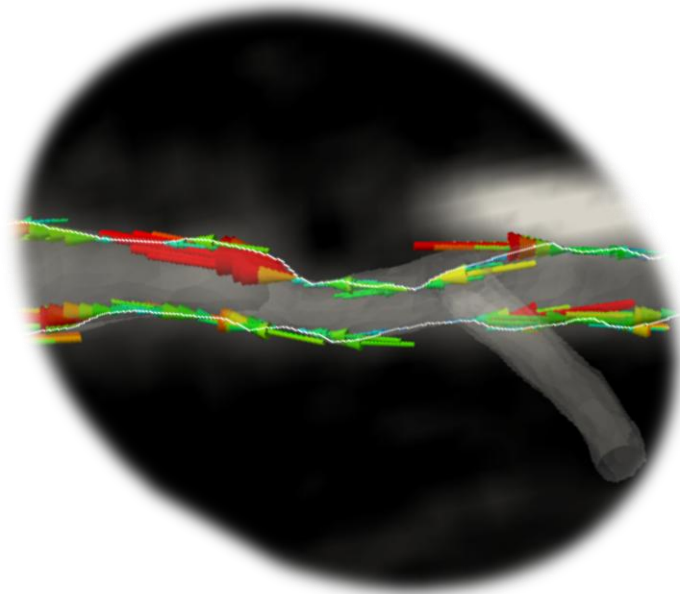
2011-04 CT, Asymptomatic



2012-06 Acute MI



APS	
Upstream	9960 dyne/cm ²
Downstream	1740 dyne/cm ²

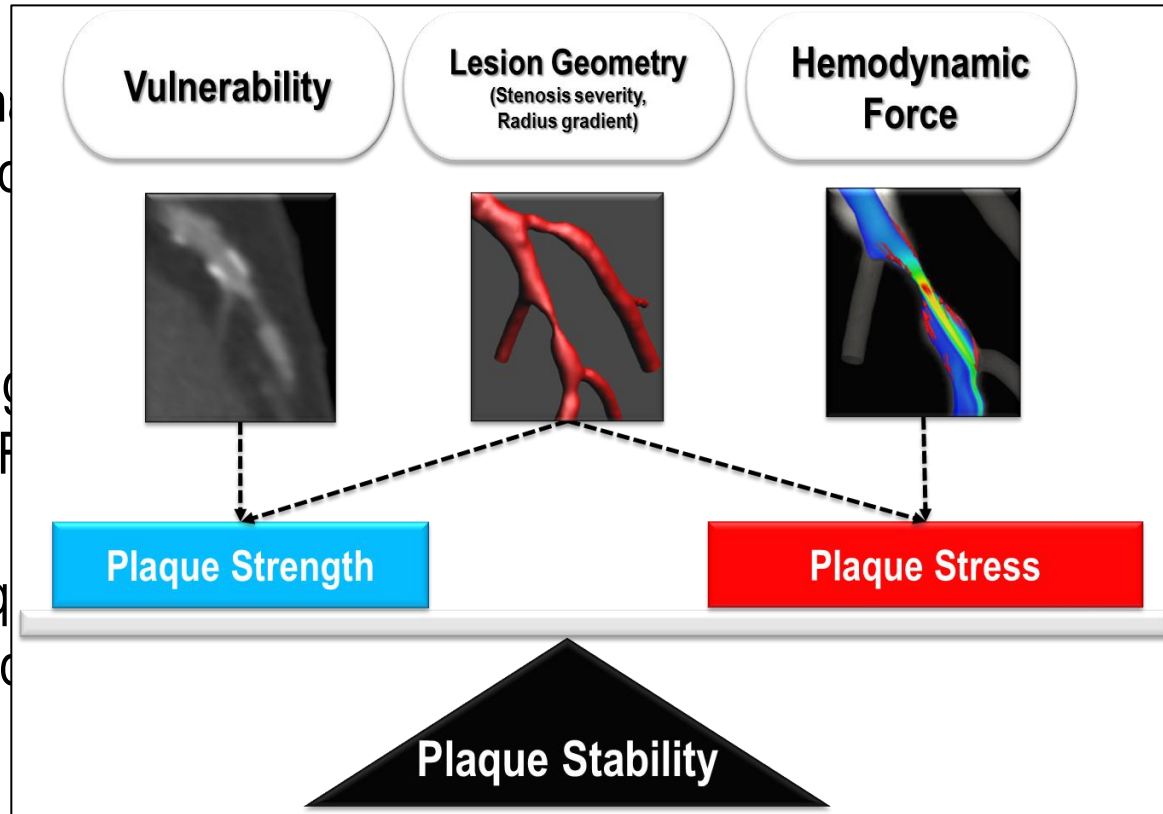


Conclusion

- Hemodynamic parameters can be measured non-invasively using coronary CT angiography.

- Very high pressure gradient exists between proximal and distal coronary artery.

- Axial plaque properties can be measured non-invasively using CT angiography.



non-invasively
S.

determined by
the link

and can

- Clinical application of these non-invasive hemodynamic parameters can be helpful to assess the future risk of plaque related clinical events.